

# Different surface topography of dental implant

Viritpon Srimaneepong D.D.S., Grad Dip, MD. Sc.

Department of Prosthodontics, Faculty of Dentistry, Chulalongkorn University

#### Abstract

In order to achieve the osseointegration, the surface of endosseous is considered as one factor determining the formation of bone-implant interface. Commercially pure (Cp) titanium implant has been widely to restore the missing teeth, however, nowadays there are many different surface treated implants in dentistry. They have shown the various clinical success and failure rates. Although the high success rate of using Cp machined titanium implant is well documented, the rough surface implant has also been shown to have a crucial role on the osseointegration. Rough surface can be created by coating with hydroxyapatite, titanium or by removing titanium surface with sandblasting or acid-etching. There are many studies shown that rough surface not only accelerates bone-implant formation but also increases removal torque. However, more clinical studies are required to prove theses benefits. (CU Dent J 2001;24:51-6)

Key words: osseointegration; surface treated implant

#### Introduction

Since 1960s, endosseous implants have been used in human, there are many evidence to show the high successful clinical employment of implant.<sup>1-5</sup> However, the successful implants not only establish osseointegration but also have to maintain the achieved osseointegration. There are many dental implant companies in the market to provide the varieties of implant systems to satisfy the practitioners' needs. There is also a lot of extrapolation between different implant systems. However, it is not possible to say that one implant will provide the same results as another one just because it looks the same. Moreover, when it comes to serve the increasing needs of implant dentistry, the shorter procedure or time will play an even increasing role. From the conventional two-stage procedure (submerged implantation) to one-stage procedure (nonsubmerged implantation), the one-step procedure has been proved successfully,<sup>1,6,7</sup> To shorten the healing time, osseointegration has to be

achieved as soon as possible. Although Commercially pure (Cp) titanium has been demonstrated to be a material with very good biocompatibility, the characteristics of rough surfaced implant have shown to have influence on bone integration of titanium implants.<sup>8,9</sup> The main objective of different surface treatment is to rough surface to improve osseointegration. Thus, the researchers have been developing the different surface treatment on implant to accelerate the osseointegration to meet the practitioners's needs. This article is, therefore, to review the different surface topography of dental implants and their surface characteristics.

# **Review of the literatures** Machined surface

Of the many different metals used in implantology, titanium has been shown to be very good biocompatibility. Titanium is used either as the pure titanium (99.75%) or as titanium alloy (T6A14V). Titanium is non-noble

metal, protected by a passivated layer of titanium dioxide that forms spontaneously in air as well as in water. According to the Branemark's concept on "osseointegration", it should be direct contact between viable bone and implant surface without inter-posing soft tissue layer. However, many histological studies have shown that there is attachment between the implant surface oxide layer and the adjacent epithelium. Hemidesmosomal like structure were observed along the epithelial cell membrane adjacent to implant surface. This attachment is mediated by glycoprotien similar to that seen between epithelium and natural teeth.<sup>10-14</sup> However, the precise biological mechanism of bone-implant interface is still not clear. Even though there will be average vertical bone loss about 0.2 mm annually after the first year of service according to criteria by Smith and Zarb in 1989<sup>15</sup>, Belser and Wiskott (1999)<sup>16</sup> recently claimed that there is no integration between bone and titanium surface. They argued that the smooth surfaces will not provide adequate biomechanical coupling with the bone surrounding the implant surface as the stress range induced by a polished surface is limited. They also explained that instead the surface texture of threaded, coated or sandblasted implants generates a heterogeneous stress field around an implant in function to induce osteocytes to form new bone. However, Cp Titanium implant has been used successfully to restore the missing teeth as it can be seen from the previous studies.<sup>2-4</sup>

#### Titanium Plasma-Sprayed (TPS) surface

Plasma-Sprayed coating used to create a rough surface was first introduced by Hahn and Palich in 1970.<sup>17</sup> It has been believed that the percentage of bone-implant contact necessary to create sufficient anchorage to permit successful implant function as a load-bearing device over time. There are some Titanium Plasma-Sprayed implant system in the market such as ITI, IMZ etc. This method is to use special plasma spraving technique, as it involves forcing noble gas (Argon), Which is split into ions and electrons (plasma), through an intensely burning (15,000-20,000 °C) arc at very high speed (3,000 m/s). Ti powder (size about 50-100  $\mu$ m) is introduced in an argon gas stream at the tip of the flame and is accelerated to approximately 600 m/s as drops of molten metal to weld to the implant surface 15-20 cm away. The resulting surface layer has a thickness of about 0.03-0.05 mm and shows a roughness depth profile of about 15  $\mu$ m. Experimental studies in animals comparing between polished surface implant

by electropolishing and rough surface implants (without electropolishing) showed significantly higher removal torque for rough-surfaced implant than smooth-surfaced implants and rough surfaced implants also demonstrated an increase in bone apposition compared to polished surfaced implants.<sup>8,18</sup> It is suggested that soft tissue components attach better to smooth-polished surfaces but the rough surface is more conducive to bone attachment.<sup>19</sup> This finding has supported the previous study on Titanium Plasma-Spraying by Sutter et al. (1988) which showed that TPS implant has optimal micromorphological structure for formation of direct bonding between bone and implant surface.<sup>20</sup> The International Team of Oral Implantology (ITI®) had successfully used implants with TPS surface treatment and it revealed that non-submerged ITI implant could achieve the success rates above 90% for observation period up to 8 years.<sup>1</sup>

#### Sandblasted surface

Instead of changing from the smooth implant surface to the rough surface by adding material, it can be done by removing material from the smooth surface for example sandblasting, or acid-etching treatment. The advantages of these techniques are that there is no contamination, and they also increase surface area and mechanical interlocking. Wennerberg et al. (1998) used custom "split" implants in animals with one side being a machined surface and the other side blasted with three sizes (25, 75, 250  $\mu$ m) of aluminum oxide (AI<sub>2</sub>O<sub>2</sub>) particles. They found that blasted surface demonstrated more bone contact to the implant surface than the smooth surface implant. Moreover, histomorphometric analysis showed surface implant blasted with 75  $\mu$ m AI2O3 particles demonstrated greater bone-implant contact than machined surface or ones blasted with 25 or 250  $\mu$ m AI<sub>2</sub>O<sub>3</sub> particle.<sup>21</sup>

## Acid-etched surface.

Apart from sandblasting technique, acid etching is another way to create rough surface. Usually, the acid used to attack implant surface is HCL/H<sub>2</sub>SO<sub>4</sub>. Recently, ITI<sup>®</sup> has introduced another surface treated implant "SLA<sup>TM</sup>" (Sand-blasted, Large grit, Acid-etched) into the market. The SLA surface has a characteristic of double roughness. The macro roughness is achieved by the large-grit sand-blasting and the micro roughness is created by acid etching. The company also claimed that the prosthetic restoration can be started within 6 weeks after the implants placement in the patients with

adequate bone. This means that it is going to shorten healing for the patient by initial speed of integration. We still need long-term study to improve the benefit of this surface treatment. Although one experimental study showed that SLA implants had a significantly higher bone-implant contact than TPS or sandblasted implants. Probably the acid not only attacked the titanium surface creating secondary roughness, but also removed the remaining grit particles of aluminum oxide embedded in the titanium surface.<sup>8</sup> Apart from TPS surface implant, 3i implant innovation<sup>®</sup> has introduced acid-etched surface implant, "Osseotite". The machine implant surface is subjected to acid-etching with  $HCL/H_2SO_4$ . The advantages of acid-etched surfaced implant are free contaminants, surface area compared to machined surface, and no coating compared to HAcoated or TPS-coated implants. Recently, one-year human experimental study<sup>22</sup> showed that the acid-etched surface (Osseotite) implant achieved earlier and higher bone to implant surface than did the machined surface implants. This in turn allowed the practitioners to start prosthetic works earlier (Early loading) instead of waiting for 3-6 months as conventional implant protocols. This study showed the high cumulative survival rates of osseotite of 98.5% at 12.6 months. However, it was 1 year study so more long-term study may be required on this protocol.

#### Hydroxyapatite coated surface

The most common ceramic used to coat the implant surface is hydroxyapatite (HA). It has been postulated that hydroxyapatite would lead to accelerated osseous healing as well as overall improvement of the interface area between bone and implant. There are controversial studies on this type of surface treated implant. The coatings contain both amorphous glassy and crytalline components and can be dense or porous. A dense coating is supposedly higher in strength and lower in solubility. It is recommended that the coating have even thickness 50-100  $\mu$ m and not obliterate surface geometry. The tensile strength of the coating to the metal is reported to be 40-80 MPa and shear strength is 10-20 MPa. Due to characteristic of ceramic material, the brittle nature is an undesirable property so it will be difficult to fabricate the thick section and to control the even thickness.<sup>23</sup> HA-coated implants have found that there was higher percentage of direct bone contact compared with uncoated cp titanium implants, titanium-coated implants or SLA implants.<sup>8,23,24</sup> HA is one of the most

biocompatible material. It has been shown to improve the rate and strength of initial osseointegration. HAcoated implant demonstrates osseoconductive property with formation of new bone contact. However, it was found that there was sign of resorption of HA-coated implant<sup>8</sup> which was contrast to a study by Block et al.<sup>25</sup> Study by Block et al. disputed previous studies and showed that the HA-coating did not show significant resorption after 9-year placement. Another retrospective study by Wheeler has shown that even though HA-coated implants had higher initial survival rate than TPS implants, after 4 year the HA-coated implant survival rates became significantly lower than TPS implants. HA-coated implants had cumulative survival rate of only 77.8% after 8 years compared to 92.7% of TPS implants. He claimed that the long-term prognosis of HA-coated implants was probably due to one of the problem of inflammatory breakdown around implants.<sup>26</sup> However, the difference in the pattern of bone contact between HA-coated implant cp Titanium has been investigated yet. One postmortem histologic study by Rohrer et al.<sup>27</sup> revealed that even though the percentage of the bone contact was higher on the mandible cp Titanium implants, compared to HA-coated implants in maxilla (56.4% VS 47%), bone contact was more uniform and solid on the maxillary HA-coated implants, similar to the study by Block et al.<sup>25</sup> They claimed that there was much more marrow in the mandible with cp Titanium implants than in maxilla with HA-coated implants. However, this investigation was done in one patient and also compared between mandible and maxilla which have different bone characteristic but it has shown some interesting finding which encourages the researchers to study more before drawing a conclusion.

#### Discussion

The surface topography is one of the properties which are proved to have an influence on the osseointegration. Although the smooth surface of dental implant has been generally accepted, it is not successful in every quality and quantity of bone. Thus, developing surface topography is necessary to improve the property of dental implant and to increase the success rate in implant dentistry. A few *in vitro* and *in vivo* studies have indicated that soft tissues interact better with smooth polished titanium surfaces, whereas rough titanium surfaces tend to promote bone tissue formation and osseointegration.<sup>8,19,28,29</sup> It can be seen that the interface reactions between metallic implants and the various surrounding tissues play an important role in the success of dental implant. There are many techniques to create the rough surface of dental implant as previous mention. By using SEM, polished surface titanium implant has roughness about 81 nm, whereas the sandblasted and acid-etched surface showed higher degree of roughness. Acid-etched surface showd roughness around 2100 nm and sandblasted/acid-etched surface showed roughness 3600 nm. Moreover, when investigating on the chemical composition and the wettability properties of titanium surface, it was seen that the surface treatments (acidetched, sandblast or plasma-spray) still preserved the properties of titanium native oxide layer compared to polished surface titanium.<sup>30</sup> However, the practitioners should consider the properties of each dental implant systems that have been treated with different techniques. Even though the HA-coated implant had shown the high rate of early bone-implant formation<sup>23,26</sup>, it has also been shown that they might be related to periimplantitis.<sup>31,32</sup> Whereas to shorten the healing period time, the rough surface dental implant has been used as we can seen in many studies on early or immediate implantation.<sup>22,33,34</sup> However, they are only short-term studies. Thus, before definitive conclusion can be drawn about superiority of these development, more long-term clinical studies are required.

#### Conclusion

Although the long-term clinical success of Cp titanium is well documented, the importance of surface characteristic and topography cannot be underestimated and further researches should be carried on to increase the success rate in implant dentistry.

# References

Buser D, Mericske-Stern R, Bernard JP, Behneke A, Behneke N, Hirt HP, et al. Long-term evaluation of non-submerged ITI implants. Part 1: 8-year life table analysis of a prospective multi-center study with 2359 implants. Clin Oral Implants Res 1997;8:161-72.

Adell R, Lekholm U, Rockler B, Branemark Pl. A 15-year of osseointegrated implants in the treatment of the edentulous jaw. Int Oral Surg 1981;10:387-416.

- Lindquist LW, Carlsson GE, Jemt T. A prospective 15-year follow-up study of mandibular fixed prostheses supported by osseointegrated implants. Clin Oral Implants Res 1996;7:329-36.
- Henry PJ, Bower RC, Wall CD. Rehabilitation of the edentulous mandible with osseointegrated dental implants: 10 years follow-up Aust Dent J 1995;40:1-9.
- 5. Jemt T. Failure and complications in 391 consecutively inserted fixed prostheses supported by Branemark implants in Edentulous

Jaws: A study of treatment from the time of prosthesis placement to the first annual checkup. Int Oral Maxillofac Implants 1991; 6:270-76.

- Bernard JP, Belser UC, Martinet JP, Borgis SA. Osseointegration of Branemark fixture using a single-step operating technique: A preliminary prospective one-year study in the edentulous mandible. Clin Oral Implants Res 1995;6:122-9.
- Collaert B, DE Bruyn H. Comparison of Branemark fixture integration and short-term survival using in completely and partially edentulous mandibles. Clin Oral Implants Res 1998;9:131-5.
- Buser D, Schenk RK, Steinemann S, Fiorellini JP, Fox CH, Stich H. Influence of surface characteristics on bone integration of titanium implants. A histomorphometric study in miniature pigs. J Biomed Mater Res 1991;25:889-902.
- Weinlaneder M, Kenney EB, Lekovic V, Beumer J, May PK, Lewis S. Histomorphometry of bone apposition around three types of endosseous dental implants. Int J Oral Maxillofac Implants 1992;7:491-6.
- Listgarten MA, Lai CH. Ultrastructure of the intact interface between an endosseous epoxy resin dental implant and the host tissue. J Biol Buccale 1975;3:13-28.
- 11. James RA. The support systems and the pergingival defense mechanism of oral implants. J Oral Implantol 1976;6:270-9.
- 12. James RA. Peri-implant considerations. Dent Clin North Am 1980;24:415-20.
- Gould TRL, Brunette DM, Westbury L. The attachment mechanisms of epithelial cells to titanium in vitro. J Periodont Res 1981;16:611-6.
- 14. Donley TG, Gillette WB. Titanium endosseous implant-soft tissue interface: a literature review. J Periodontol 1991;62:153-60.
- 15. Smith DE, Zarb GA. Criteria for success of osseointegrated endosseous implants J Prosthet Dent 1989;62:567-72.
- 16. Wiskott HWA, Belser UC. Lack of integration of smooth titanium surface: a working hypothesis based on strains generated in the surrounding bone. Clin Oral Implants Res 1999;10:429-44.
- Hahn H, Palich W. Preliminary evaluation of porous metal surfaced titanium for orthopedic implants. J Biomed Mater Res 1970;4:571-7.
- Carlsson L, Rostlund T, Albrektsson B, Albrektsson T. Removal torques for polished and rough titanium implants. Int J Oral Maxillofac Implants 1988;3:21-4.
- Cochran DL, Simpson J, Weber HP, Buser D. Attachment and growth of periodontal cells on smooth and rough titanium. Int J Oral Maxillofac Implants 1994;9:289-97.
- Sutter F, Schroeder A, Buser A. The new concept of ITI hollowcylinder and hollow screw implants: Part 1 Engineering and design. Int Oral Maxillofac Implants 1988;3:161-72.
- 21. Wennerberg A, Hallgren C, Johansson C, Danelli S. A histomorphometric evaluation of screw-shaped implants each prepared with two surface roughnesses. Clin Oral Implants Res 1998;9:11-9.
- 22. Lazzara RJ, Porter SS, Testori R, Galante J, Zetterqvist L. A Prospective Multicenter Study Evaluating Loading of Osseotite Implants Two Months after placement:one-year results. J Esthet Dent 1998;10:280-9.
- Gottlander M, Albrektsson T, Carlsson LV. A histomorphometric study of unthreaded Hydroxyapatite-coated and titanium-coated implants in rabbit bone. Int J Oral Maxillofac Implants 1992; 7:485-90.

- 24. Gottlander M, Albrektsson T. Histomorphometric studies of hydroxyapatite-coated and uncoated cp Titanium thread implants in bone. Int J Oral Maxillofac Implants 1991;6:339-404.
- Block MS, Finger IM, Misiek DJ. Histologic examination of a hydroxyapatite-coated implant nine years after placement. J Oral Maxillofac Surg 1996;64:1023-6.
- 26. Wheeler SL. Eight-year clinical retrospective study of titanium plasma-sprayed and hydroxyapatite-coated cylinder implants. Int J Oral Maxillofac Implants 1996;11:340-50.
- Rohrer MD, Sobczak RR, Prasad HS, Morris HF. Postmortem hislogic evaluation of mandible titanium and maxillary hydroxyapatite-coated implants from 1 patient. Int J Oral Maxillofac Implants 1999;14:579-86.
- Cheroudi B, Gould TRL, Bruntte DM. A light and electron microscope study of the cells attached to titanium-coated percutaneous implants. J Biomed Mater Res 1991;25:289-97.
- Bowers KT, Keller JC, Randolph BA, Wick DG, Michael CM. Optimization of surface morphology for enhanced osteoblast responses in vivo. Int J Oral Maxillofac Implants 1992;7:302-10.
- 30. Taborelli M, Jobin M, Francois P, Vandaux P, Tonetti M,

Szmukler-Moncler S, Simpson JP, Descouts P. Influence of surface treatment developed for oral implant the physical and biological properties of titanium. I Surface characterization. Clin Oral Implants Res 1997;8:208-16.

- Teixeira ER, Sato Y, Akagawa Y, Kimoto T. Correlation between mucosal inflammation and marginal bone loss around hydroxyapatitecoated implants: a 3-year cross-sectional study. Int J Oral Maxillofac Implants 1997;12:74-81.
- Hanisch O, Cortella CA, Boskovic MM, James RA, Slots J, Wikesjo UM. Experimental peri-implant tissue breakdown around hydroxyapatite-coated implants. J Periodontol 1997;68:59-66.
- Tarnow DP, Emtiaz S, Classi A. Immediate loading of threaded implants at stage 1 surgery in edentulous arches: ten consecutive case reports with 1-to 5-year data. Int Oral Maxillofac Implants 1997;12:319-24.
- 34. Ledermann PD, Schenk RK, Buser D. Long-lasting osseointegration of immediately loaded, bar-connected TPS screws after 12 years of function: a histologic case report of a 95-year-old patient. Int J Periodontics Restorative Dent 1998;18:552-63.

# ลักษณะพื้นผิวที่แตกต่างกันของรากเทียม

## วิธิทธิ์พล ศรีมณีพงศ์ ท.บ., Grad Dip, MD. Sc

ภาควิชาทันตกรรมประดิษฐ์ คณะทันตแพทยศาสตร์ จุฬาลงกรณ์มหาวิทยาลัย

# บ**ทคัดย่อ**

ลักษณะพื้นผิวของรากเทียมเป็นหนึ่งในหลายปัจจัยที่จะช่วยส่งเสริมให้เกิดการเกาะติดระหว่างผิวของรากเทียม กับกระดูก ถึงแม้ว่ารากเทียมที่ทำขึ้นจากโลหะไททาเนียมบริสุทธิ์ทางการค้าจะถูกนำมาใช้ในการบูรณะ และซดเซย พันที่สูญหายไปมาซ้านานแล้วก็ตาม รวมทั้งได้แสดงให้ถึงอัตราความสำเร็จที่สูง แต่ปัจจุบันจะพบว่ารากเทียมได้ถูก พัฒนาให้มีลักษณะพื้นผิวที่แตกต่างกันออกไปเพื่อสนองความต้องการของทันตแพทย์ ซึ่งนอกเหนือจากรากเทียม ไททาเนียมที่มีผิวเรียบที่ถูกยอมรับอย่างกว้างขวางแล้ว รากเทียมที่มีผิวหยาบได้ถูกนำมาทดลองและใช้ รวมถึงแสดง ให้เห็นถึงผลของลักษณะของพื้นผิวรากเทียมต่อการเกาะติดระหว่างผิวของรากเทียมกับกระดูก รากเทียมสามารถ ถูกทำให้เกิดผิวที่หยาบได้โดยการเคลือบด้วยไฮดรอกซีแอปพาไทต์ หรือ ผงไททาเทียมกับกระดูก รากเทียมสามารถ ถูกทำให้เกิดผิวที่หยาบได้โดยการเคลือบด้วยไฮดรอกซีแอปพาไทต์ หรือ ผงไททาเทียมที่มีผิวหยาบนอกเหนือจากจะ เพิ่มอัตราการเกาะติดระหว่างผิวของรากเทียมกับกระดูกแล้วยังเพิ่มแรงต้านแรงบิดหมุนในห้องปฏิบัติการ อย่างไรก็ตาม ยังต้องมีการศึกษาเพิ่มเติมทางคลินิกอีกมากก่อนที่จะสรุปถึงข้อดีต่าง ๆ ของรากเทียมที่มีผิวหยาบ

(ว ทันตจุฬาฯ 2544;24:51-6)